



# Vocal Fold Movement Prediction from Neural Inputs:

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Building the Model

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# Research Question

*To what degree can a three-dimensional biomechanical vocal fold model predict the dynamics of a posturing gesture?*



# Myoelastic-Aerodynamic Theory of Phonation

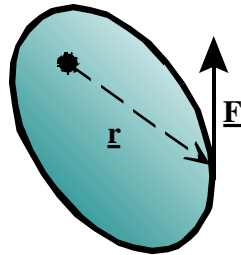
- Vocal-tract acoustics
- Laryngeal aerodynamics
- Tissue mechanics

*Configuration of the tissue*

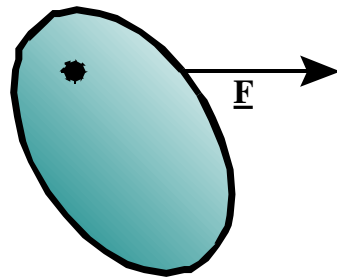
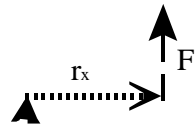
*is key to phonation.* (Murry, et al, 1998)

- ◆ Vibration
- ◆ Posturing

# Previous Posturing Models

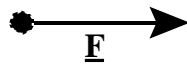


Torque =  
 $\underline{r} \times \underline{F} =$



$\underline{F}$  = Force

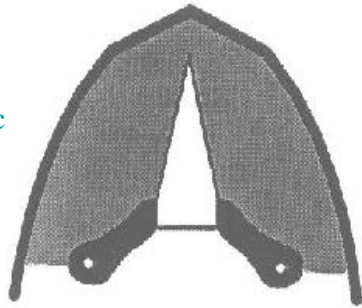
$\underline{F} = m \underline{a}$



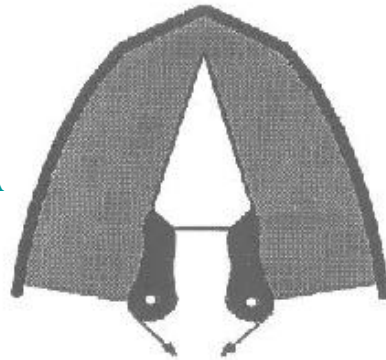
## Classical analytical model

- ◆ Ridged body mechanics
- ◆ Tissue compressibility
- ◆ Two dimensions
- ◆ Vocal fold medial shape

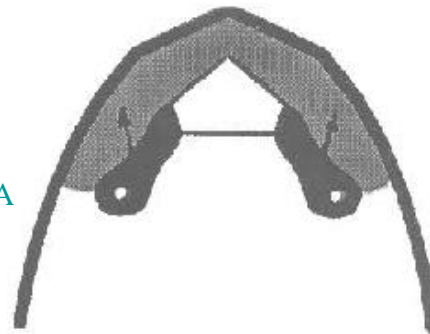
Cadaveric



Full LCA



Full TA

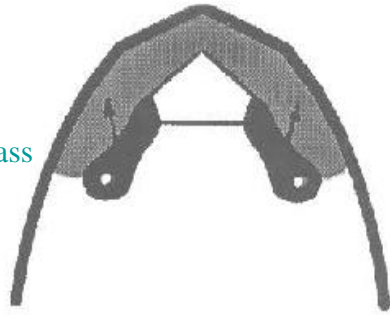


## Classical analytical model

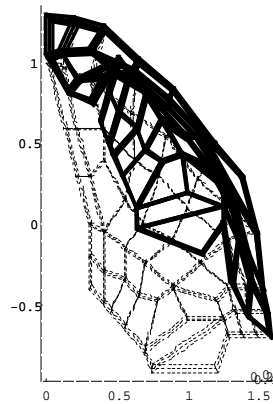
- ◆ Ridged body mechanics
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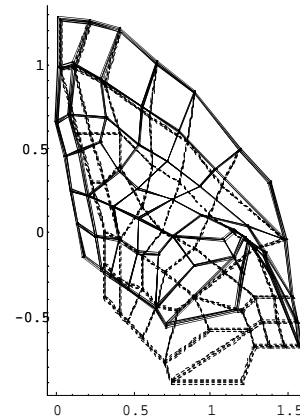
Full TA  
point mass



Full TA  
compressible



Full TA  
incompressible



## Classical analytical model

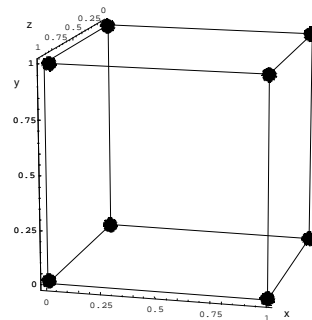
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# Finite Elements

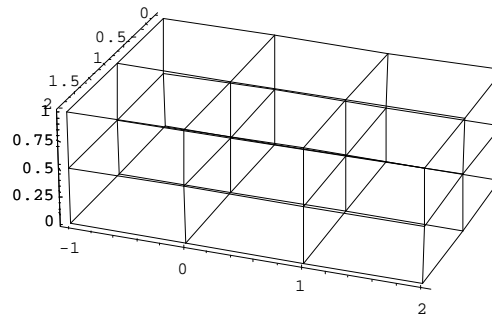
Continuum mechanics  
through finite elements

- ◆ geometry
- ◆ mechanical properties
- ◆ boundary conditions
- ◆ discretization

Hexahedral  
element

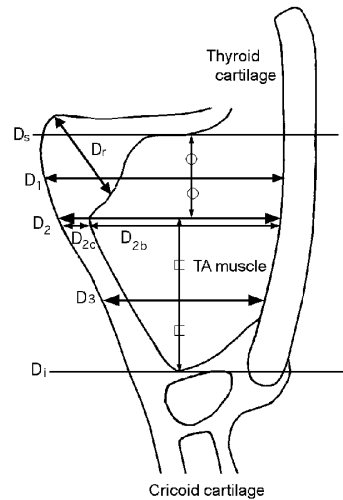


Simple  
structure

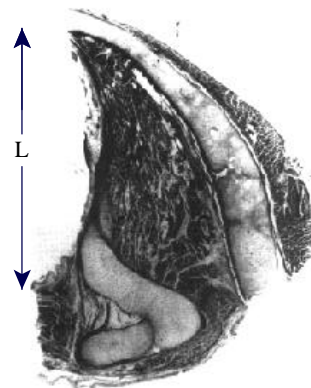


# Geometry

Rostra  
caudal



Simple  
structure



- Use existing *in vitro* data of laryngeal specimens (Eckel *et al*, 1994) and VABL data (Tayama *et al*, 1999)
- Simplify geometry of all tissue inside thyroid cartilage, including arytenoid cartilage

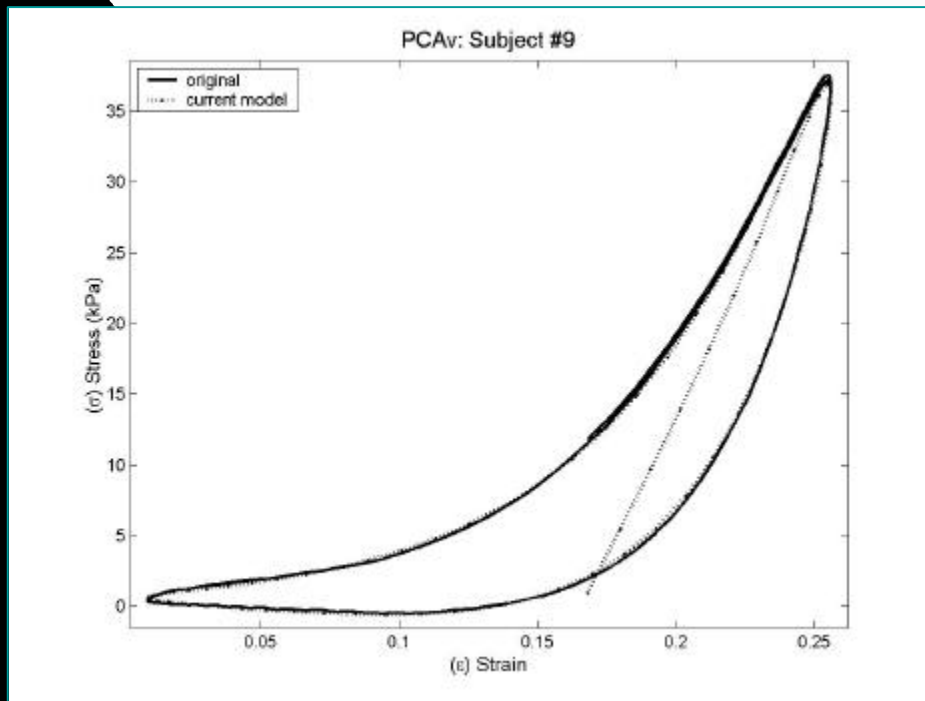
# Defining Mechanical Properties

- Develop governing equations that apply to all tissue

$$\sigma = E \epsilon \quad (\text{linear example})$$

- Identify material properties of individual tissues
  - ◆ Passive properties
  - ◆ Active properties

# Passive Properties



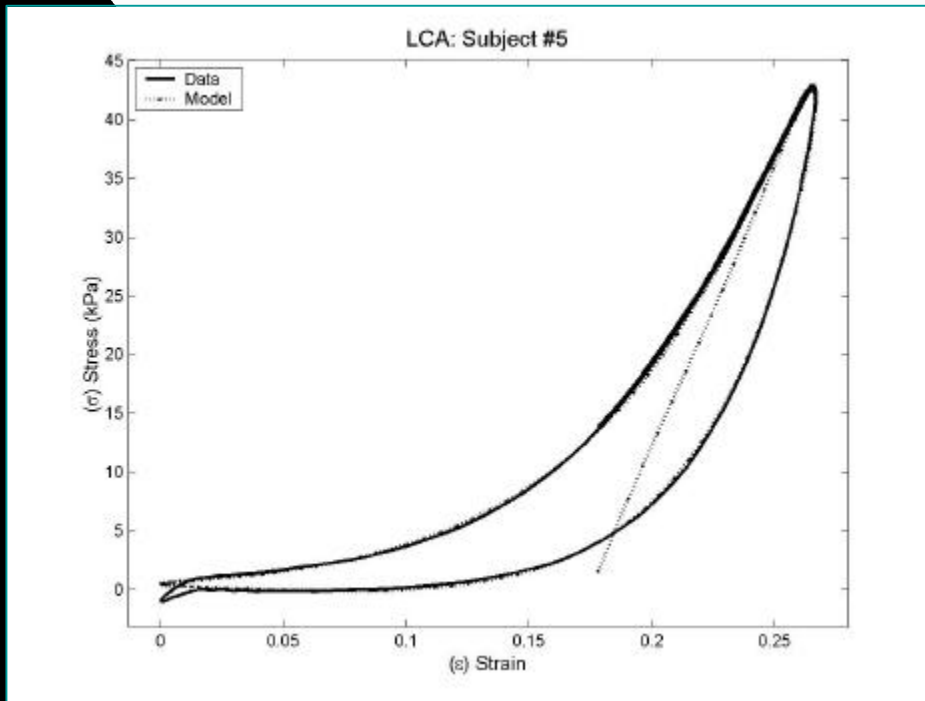
PCAv at 1hz elongation cycle

- All tissues have passive properties
- Dynamic stress-strain of IA, LCA, PCAv, PCAo (5 canine laryngeal specimen)
- Modeling these curves using a 7-parameter model

$$t_s \dot{\sigma} + \sigma = \sigma_i + \sigma_p + Et_p \dot{\varepsilon}$$

$$\sigma_p = -\frac{\sigma_o}{\varepsilon_1}(\varepsilon - \varepsilon_1) - B\sigma_2(\varepsilon - \varepsilon_2) + \sigma_2[e^{B(\varepsilon - \varepsilon_2)} - 1], \quad \varepsilon > \varepsilon_2$$

# Passive Properties



$$ERR = \sum_n (\sigma_d(n) - \sigma_m(n))^2$$

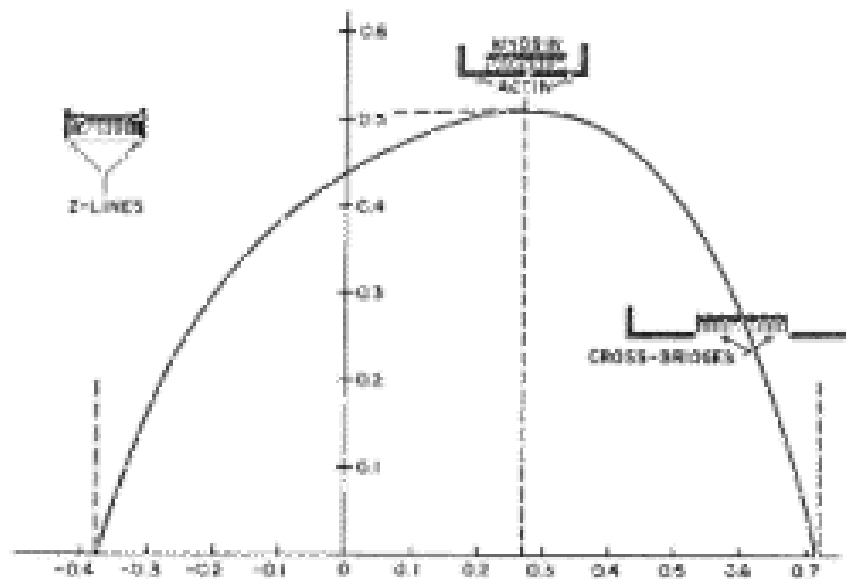
- Nelder and Mead Simplex method of optimization
- Tolerances to end optimization attempt set to 1 percent
  - ◆ trial-to-trial difference between parameters
  - ◆ trial-to-trial summed square of measured vs modeled stress

# Passive Properties- Results

Parameters' mean values, their standard deviations, and the number of contributing specimens

	IA			LCA			PCAO			PCAv		
	mean	s.d.	N	mean	s.d.	N	mean	s.d.	N	mean	s.d.	N
<b>Iteration</b>	1364	364	5	2770	1150	4	1431	480	5	3602	2249	4
<b><math>\dot{\sigma}_0</math> (Pa)</b>	1333	242	5	751	114	4	1551	396	5	818	263	4
<b><math>\dot{\sigma}_2</math> (Pa)</b>	7099	2105	5	329	224	4	6019	4754	5	28	17	4
<b><math>\ddot{a}_1</math></b>	-0.5	0	5	-0.5	0	4	-0.5	0	5	-0.5	0	4
<b><math>\ddot{a}_2</math></b>	0.00439	0.02581	5	-0.0231	0.04809	4	0.03999	0.04075	5	-0.182	0.01834	4
<b>B</b>	5.947	0.776	5	14.908	1.565	4	10.842	2.898	5	16.10	0.310	4
<b><math>t_p</math> (sec)</b>	0.09038	0.00308	5	0.09931	0.01860	4	0.08443	0.01417	5	0.1154	0.01279	4
<b><math>t_s</math> (sec)</b>	0.05058	0.00236	5	0.05429	0.01237	4	0.04843	0.00899	5	0.0612	0.00674	4

# Active Tissue Properties



$$\sigma_a = a \sigma_m f(\epsilon_y) g(\epsilon_y)$$

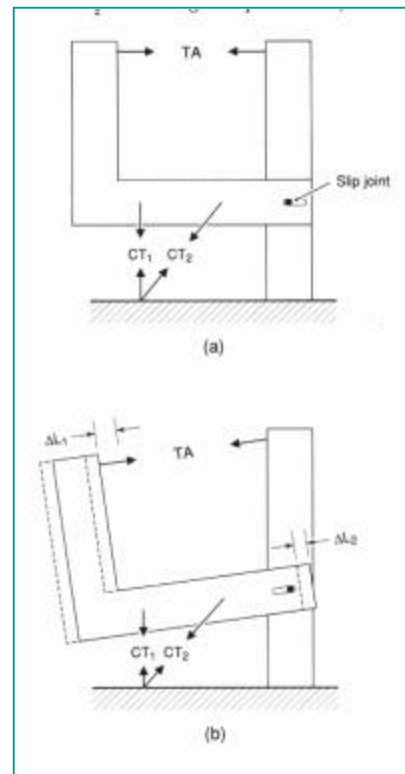
$$g(\epsilon) = \text{Max} \left[ 0, \frac{\epsilon/\epsilon_m + 1}{1 - 3\epsilon/\epsilon_m} \right] \quad \epsilon \leq 0$$

$$= \frac{9\epsilon/\epsilon_m + 1}{5\epsilon/\epsilon_m + 1} \quad \epsilon > 0$$

$$f(\epsilon) = \max \left[ 0, 1 - b(\epsilon - \epsilon_m)^2 \right]$$

- Only muscle tissues have active properties
- Assumption: total stress of muscle is superposition of its active and passive properties
- Optimize to twitch response using same scheme as before

# Boundary Conditions

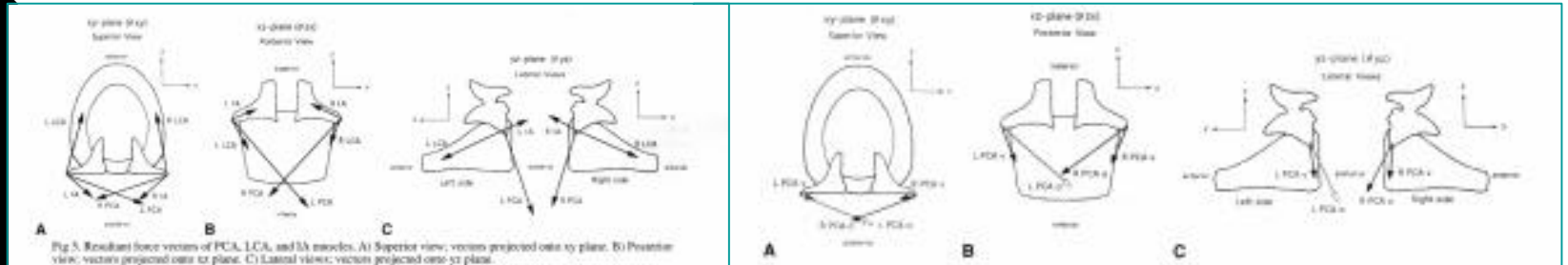


- Thyroid cartilage
  - ◆ CTJ mechanics (Titze, 1994)
- Arytenoid cartilage
  - ◆ Rocking
  - ◆ Sliding
  - ◆ Rotation (Sellars & Vaughan, 1983)
- Free medial boundary

$$\varepsilon = G(R a_{ct} + a_{ta}) + \varepsilon_0$$

Axis	X (mm)	Y (mm)	Z (mm)
Rocking	4.9	-3.8	-5.6
Sliding	9.2	-5.9	-10.8
Twisting	14.0	-21.7	23.2

# Boundary Conditions

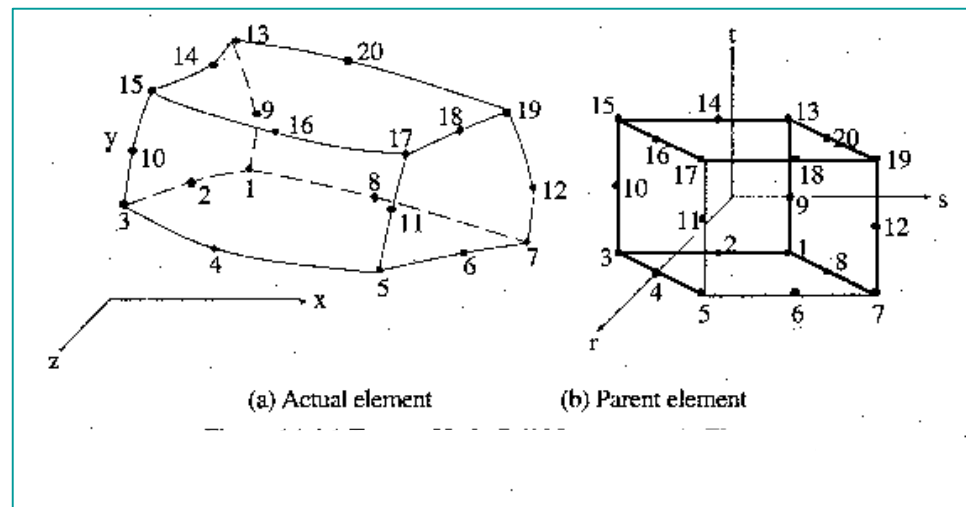


- Apply muscle stresses to origin and insert points on cartilages in appropriate directions (Mineck, *et al*, 1999)
- Quantify CAJ stiffness (Berry *et al*, 1999)

Translational	$k_x$ (N/m)	$k_y$ (N/m)	$k_\theta$ (Nm/rad)
Stiffness	91	254	0.0120

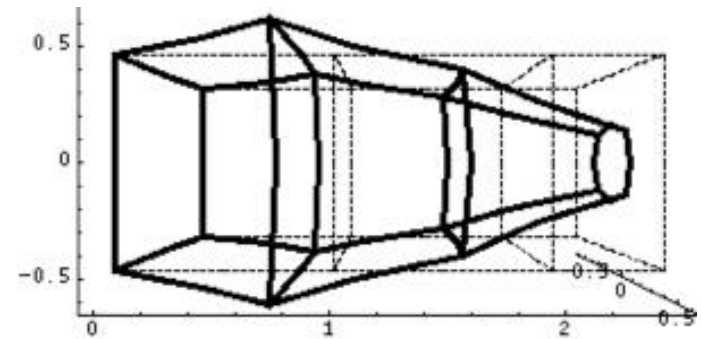
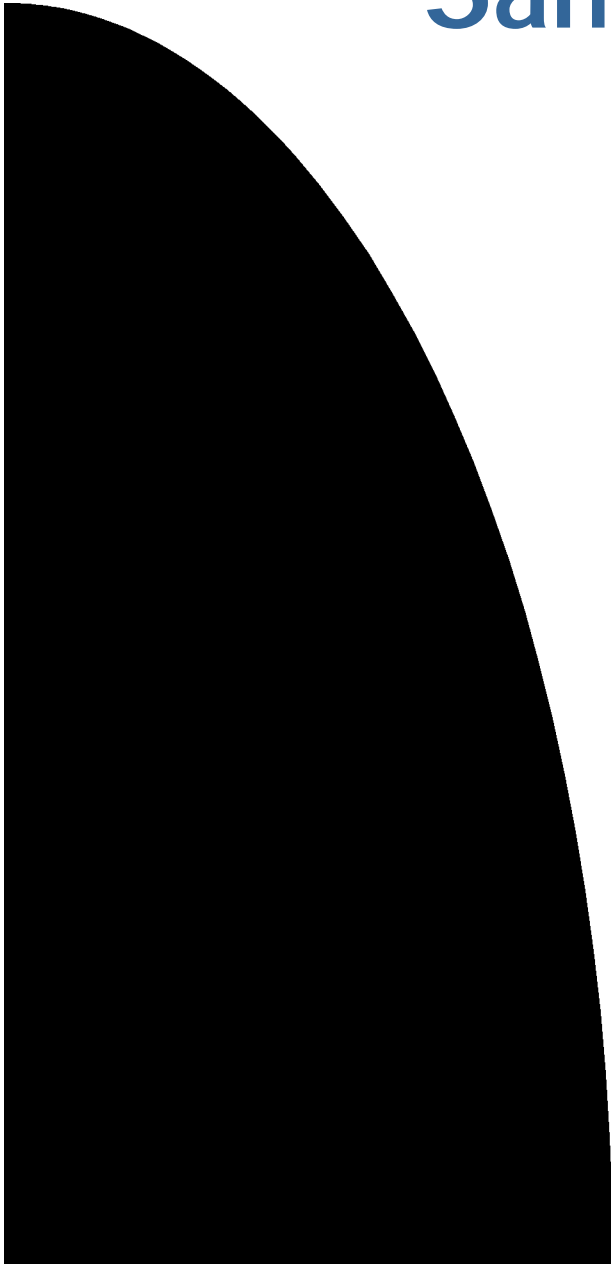
# Discretization

- Finite element analysis divides the continuum into small elements.
- Simple continuum mechanic equations approximate solutions over these small elements.

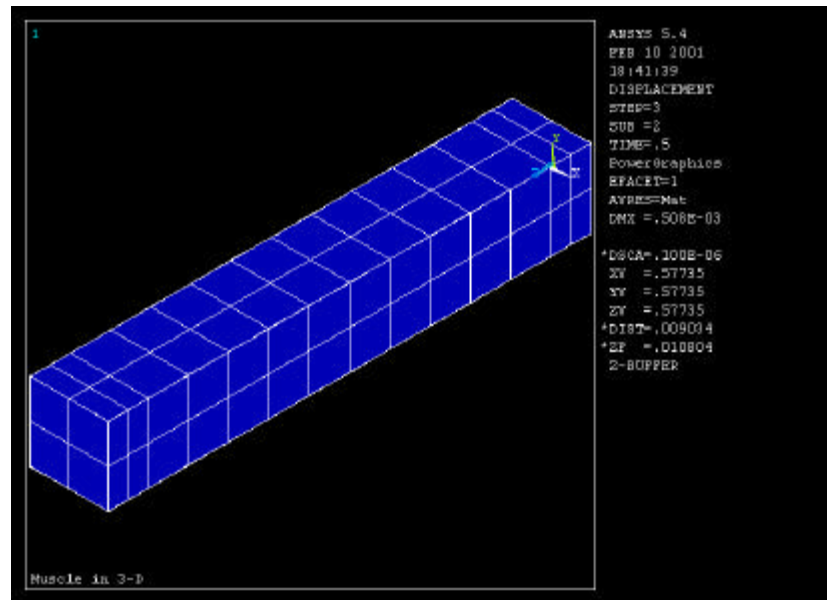


twenty node isoparametric element

# Sample Muscle

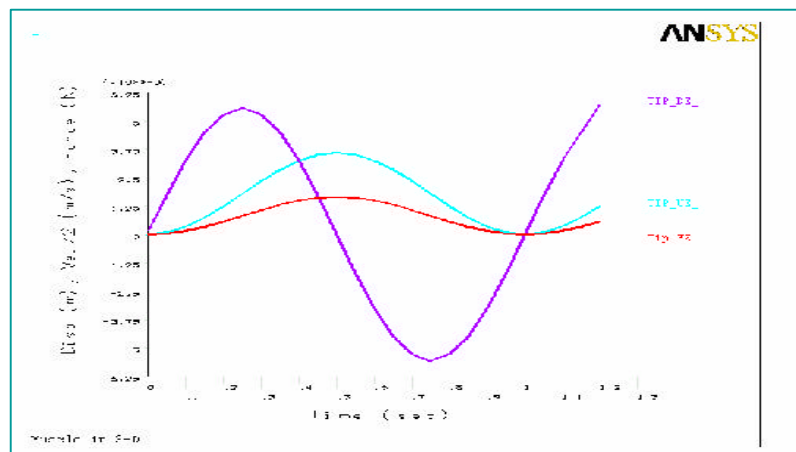
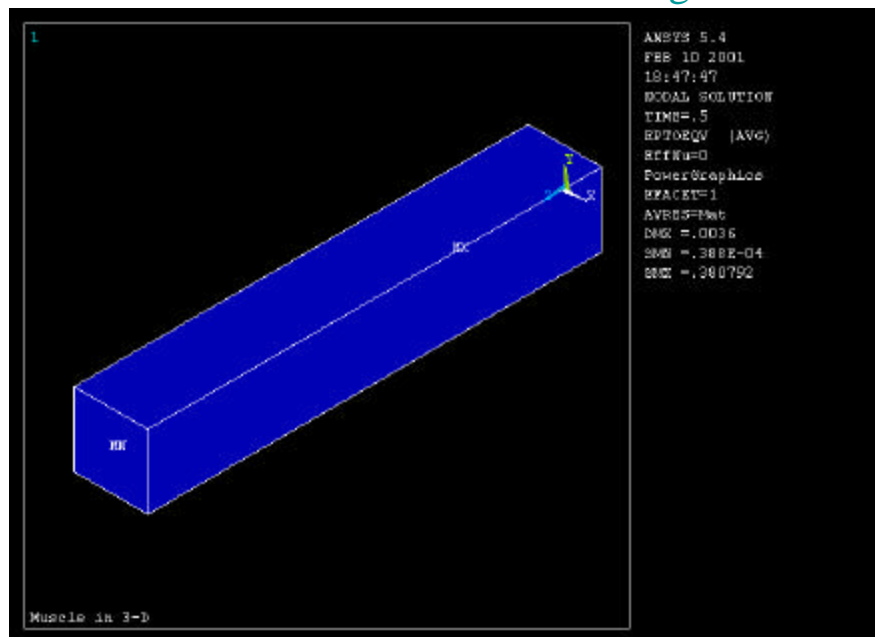


Contracted Muscle



# Sample Muscle 2

Elongated muscle

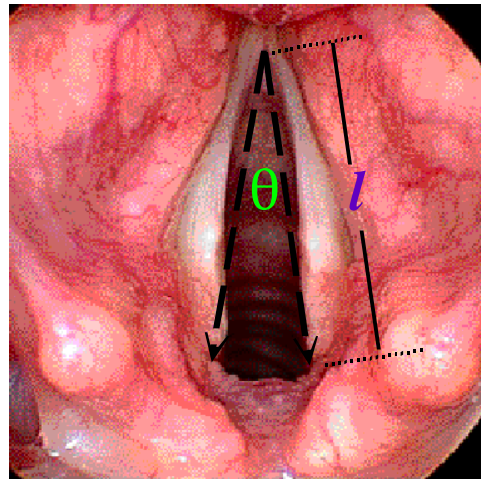


# Testing the Model

- Using a high-speed endoscope, vocal fold length glottal angle will be measured for specific postures

Posture	Assumed Muscle Activity
A quick sniff or inhalation (sniff-/i/-sniff-/i/)	the PCA will be assumed at maximum activity
A low-to-high pitch glide (fold lengthening in non-falsetto register)	CT and TA are both nearly maximum for a high pitch if the vibration is not considered a falsetto register (Titze, Luschei, and Hirano, 1989)
alternating low and high pitches	Sundberg, J. (1977), Sundberg, J. (1987).
Pressed Phonation, Cough	
A valsalva (a hard closure)	the LCA and IA will be assumed maximum

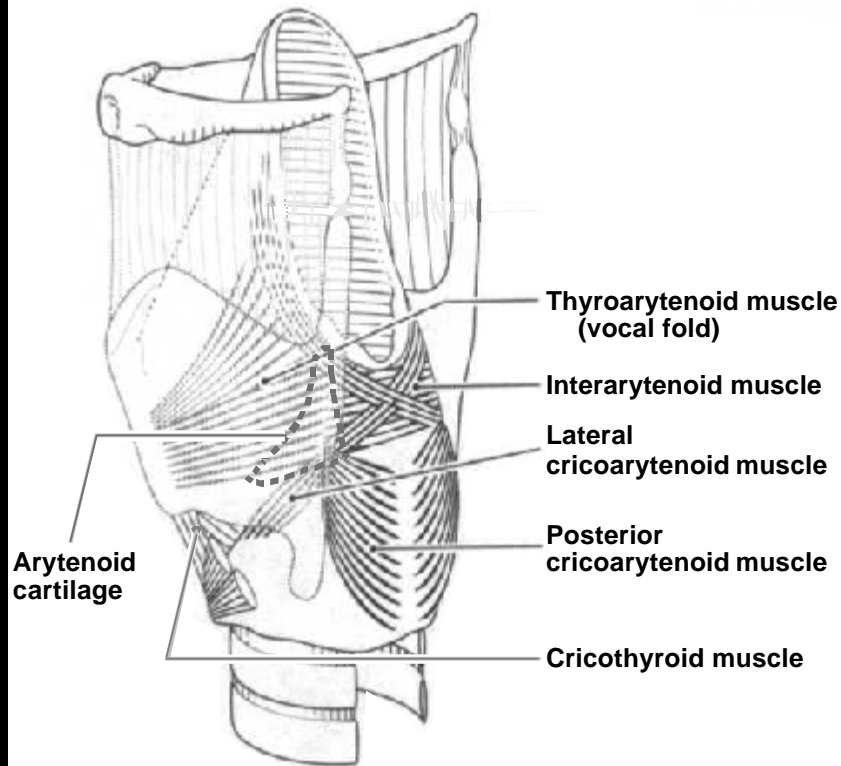
# Neurological Projections



- Muscle activities  $a$  will be obtained by fitting the results of the model to the results of the high speed endoscopy measures.

Name	Symbol	Calculation
Glottal Angle	$\theta$	
Range of Glottal Angle	$\Delta\theta$	$(\theta_2 - \theta_1)/2$
Glottal Angle Rate of Change	$\dot{\Delta\theta}$	$(\theta_2 - \theta_1)/(2 \Delta t)$
Vocal Fold Length Change	$\Delta l$	$(l - l_0)/l_0$
Vocal Fold Length Rate of Change	$\dot{\Delta l}$	$(l - l_0)/(l_0 \Delta t)$

# What is still to be done?



- Active properties are still being optimized
- High-speed endoscopic data is being taken TODAY
- *The Future?*

# Bibliography

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